

# Characterization of superparamagnetic particles with MR relaxometry: good and bad news

**Superparamagnetic particles** are used as contrast agents in cellular and molecular **Magnetic Resonance Imaging (MRI)**. Their efficiency can be predicted by a suited theoretical model. Moreover the fitting of **Nuclear Magnetic Resonance (NMR)** relaxation data by this theory provides the size and saturation magnetization of the particles. It is therefore **crucial to validate the theory** in different experimental conditions.

## 1. Relaxation induced by superparamagnetic particles

- Superparamagnetic nanoparticles = contrast agents for  $T_2$ -weighted MRI.
- Relaxation = dynamics of the proton NMR signal
  - in the direction of  $B_0$  (longitudinal relaxation, time  $T_1$ )
  - in the plane  $\perp$  to  $B_0$  (transverse relaxation, time  $T_2$ )
- Superparamagnetic relaxation  $\propto$  dipolar interaction between the huge particle magnetic moment and those of (water) protons + time modulation by the diffusion of (water) protons.
- $\Rightarrow$  drastic decrease of  $T_2$  and slighter decrease of  $T_1$  : faster relaxation!
- $\Rightarrow$  Relaxation model developed by Roch et al (1) in the **Motional Averaging Regime (MAR)**.

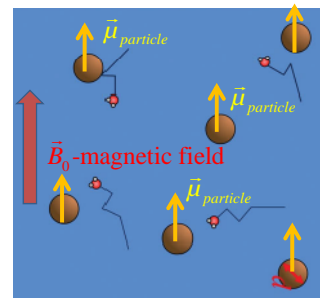


Figure 1: sketch of NMR relaxation of water protons induced by magnetic particles

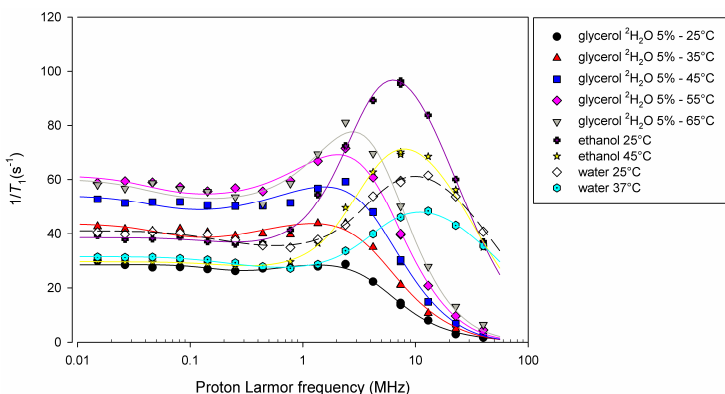


Figure 2:  $T_1$  NMRD profiles of different suspensions of USPIO particles,  $[Fe] = 1.49$  mM. The lines are fittings by the relaxation model of Roch [1].

- Theoretical validity of the Roch model depends on:
  - the radius  $R$  and magnetization  $Mv$  of the particles,
  - the diffusion properties of protons in the particles suspension,
- $\Rightarrow$  2 relevant parameters:
  - the proton diffusion time  $\tau_D = R^2/D$  where  $D$  is the diffusion coefficient of protons.
  - the Larmor frequency shift at the equator of the particle,  $\Delta\omega = \gamma\mu_p M_v/3$ .
- MAR is applicable when  $\Delta\omega\tau_D < 1$   $\rightarrow$  Roch model is valid when  $\Delta\omega\tau_D < 1$ .

## 2. Questions

- Is the theory valid outside the MAR? Change  $R$ ,  $Mv$  (2) or **Diffusion coefficient**
  - $\Rightarrow$  change the temperature, solvent or both (Fig. 2)
- Is the theory valid for  $T_1$  and  $T_2$  simultaneously?
  - $\Rightarrow$  Simultaneous fitting of  $T_1$  and  $T_2$  data (Fig. 3)
- Is the theory valid for another nucleus ( $^2H$ )?
  - $\Rightarrow$  Measurement and fitting for a suspension of particles in heavy water (Fig. 4).
- Samples = Suspensions of Ultra Small Particles of Iron Oxide (USPIOs):
  - $R = 3.76$  nm ( $\sigma = 0.2$ ) and  $Mv = 330000$  A/m.
- Experimental data = values of  $T_1$  and  $T_2$  at different magnetic fields = Nuclear Magnetic Relaxation Dispersion (NMRD) curve.

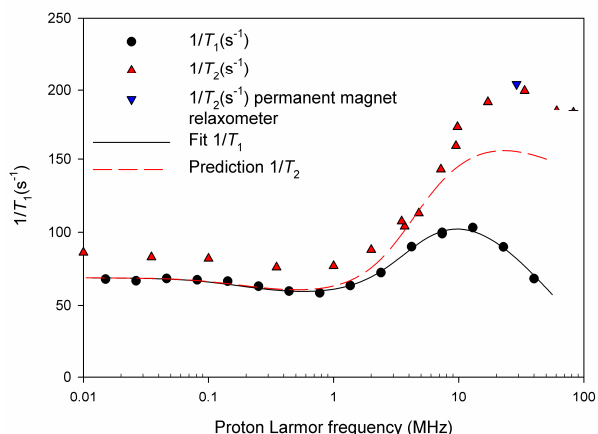


Figure 3:  $T_1$  and  $T_2$  NMRD profiles of an aqueous suspension of USPIO particles at 25°C,  $[Fe] = 2.5$  mM. The plain line is a fitting of the  $T_1$  data while the dashed line is the prediction of  $T_2$  using the parameters obtained from the  $T_1$  fitting.

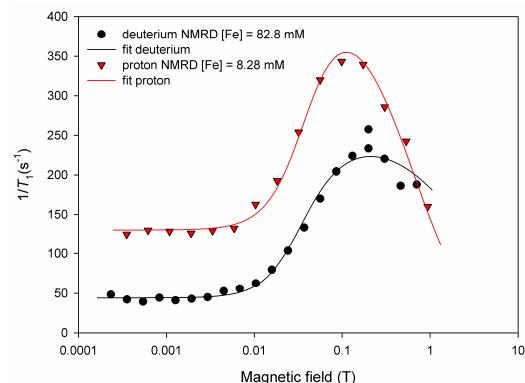


Figure 4:  $^2H$  and  $^1H$   $T_1$  NMRD profiles of 20 nm clusters of USPIO particles at 37°C. Line are fittings by the Roch model.

## 2. Answers

Good news 😊

- The Roch model allowed to fit the  $T_1$  data even outside the MAR (up to  $\Delta\omega\tau_D = 187$ ).
- $R$  values obtained from the fittings (from 4 to 6nm) consistent with the actual radius value.
  - $\Rightarrow$  determination of radius still valid even outside the MAR.
- $Mv$  values always smaller, when outside the MAR, than the actual magnetization value.
  - $\Rightarrow$  The  $Mv$  values are not reliable outside the MAR.
- $^2H$  NMRD can be fitted by the Roch theory : dipolar relaxation instead of quadrupolar relaxation because of the enormous magnetic moment of the particle.

Bad news 😞

- Impossible to fit simultaneously the  $T_1$  and  $T_2$  NMRD profile (while in the MAR condition).

## 4. References

1. Roch et al. Journal of Chemical Physics 110, 11, (1999). 2. Vuong et al. Advanced Healthcare Materials 1, 4 (2012). 3. Gossuin et al. Nanotechnology 27, 155706 (2016).